Integrated computational physics and numerical optimization

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Optimize physics

Optimize numerics

Optimize physics

Optimize numerics

PDE optimization is ubiquitous in science and engineering

Design: Find system that optimizes performance metric, satisfies constraints





Aerodynamic shape design of automobile



Optimal flapping motion of micro aerial vehicle

PDE optimization is ubiquitous in science and engineering

Inverse problems: Infer the problem setup given solution observations





Material inversion: find inclusions from acoustic, structural measurements Source inversion: find source of contaminant from downstream measurements



Full waveform inversion: estimate subsurface of crust from acoustic measurements

Goal: Find the solution of the unsteady PDE-constrained optimization problem

$$\begin{array}{ll} \underset{\boldsymbol{U}, \ \boldsymbol{\mu}}{\text{minimize}} & \mathcal{J}(\boldsymbol{U}, \boldsymbol{\mu}) \\ \text{subject to} & \boldsymbol{C}(\boldsymbol{U}, \boldsymbol{\mu}) \leq 0 \\ & \frac{\partial \boldsymbol{U}}{\partial t} + \nabla \cdot \boldsymbol{F}(\boldsymbol{U}, \nabla \boldsymbol{U}) = 0 \quad \text{in} \quad v(\boldsymbol{\mu}, t) \end{array}$$

PDE solution design/control parameters

 $\operatorname{constraints}$

$$\begin{split} & \boldsymbol{\mu} \\ & \mathcal{J}(\boldsymbol{U},\boldsymbol{\mu}) = \int_{T_0}^{T_f} \int_{\boldsymbol{\Gamma}} j(\boldsymbol{U},\boldsymbol{\mu},t) \, dS \, dt \\ & \boldsymbol{C}(\boldsymbol{U},\boldsymbol{\mu}) = \int_{T_0}^{T_f} \int_{\boldsymbol{\Gamma}} \mathbf{c}(\boldsymbol{U},\boldsymbol{\mu},t) \, dS \, dt \end{split}$$

 $\boldsymbol{U}(\boldsymbol{x},t)$

Optimizer

Primal PDE

Dual PDE









Highlights of globally high-order discretization

Arbitrary Lagrangian-Eulerian formulation: Map, $\mathcal{G}(\cdot, \mu, t)$, from physical $v(\mu, t)$ to reference V

$$\left. \frac{\partial \boldsymbol{U}_{\boldsymbol{X}}}{\partial t} \right|_{\boldsymbol{X}} + \nabla_{\boldsymbol{X}} \cdot \boldsymbol{F}_{\boldsymbol{X}}(\boldsymbol{U}_{\boldsymbol{X}}, \ \nabla_{\boldsymbol{X}}\boldsymbol{U}_{\boldsymbol{X}}) = 0$$

Space discretization: discontinuous Galerkin

$$M \frac{\partial u}{\partial t} = r(u, \mu, t)$$

Time discretization: diagonally implicit RK

$$u_n = u_{n-1} + \sum_{i=1}^{s} b_i k_{n,i}$$
$$M k_{n,i} = \Delta t_n r (u_{n,i}, \mu, t_{n,i})$$

Quantity of interest: solver-consistency

$$F(\boldsymbol{u}_0,\ldots,\boldsymbol{u}_{N_t},\boldsymbol{k}_{1,1},\ldots,\boldsymbol{k}_{N_t,s},\boldsymbol{\mu})$$



Mapping-Based ALE



DG Discretization



Butcher Tableau for DIRK

Fully discrete output function i.e., either **objective** or a **constraint**

$$F(\boldsymbol{\mu}) = F(\boldsymbol{u}_0, \dots, \boldsymbol{u}_n, \boldsymbol{k}_{1,1}, \dots, \boldsymbol{k}_{N_t,s}, \boldsymbol{\mu})$$

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Total derivative with respect to parameters μ

$$DF = \frac{\partial F}{\partial \boldsymbol{\mu}} + \sum_{n=0}^{N_t} \frac{\partial F}{\partial \boldsymbol{u}_n} \frac{\partial \boldsymbol{u}_n}{\partial \boldsymbol{\mu}} + \sum_{n=1}^{N_t} \sum_{i=1}^s \frac{\partial F}{\partial \boldsymbol{k}_{n,i}} \frac{\partial \boldsymbol{k}_{n,i}}{\partial \boldsymbol{\mu}}$$

However, the sensitivities, $\frac{\partial u_n}{\partial \mu}$ and $\frac{\partial k_{n,i}}{\partial \mu}$, are expensive to compute, requiring the solution of n_{μ} linear evolution equations

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Adjoint method

Alternative method for computing DF that does not require sensitivities

Dissection of fully discrete adjoint equations

- Linear evolution equations solved backward in time
- **Primal** state/stage, $u_{n,i}$ required at each state/stage of dual problem
- Heavily dependent on **chosen ouput**

$$\boldsymbol{\lambda}_{N_{t}} = \frac{\partial \boldsymbol{F}}{\partial \boldsymbol{u}_{N_{t}}}^{T}$$
$$\boldsymbol{\lambda}_{n-1} = \boldsymbol{\lambda}_{n} + \frac{\partial \boldsymbol{F}}{\partial \boldsymbol{u}_{n-1}}^{T} + \sum_{i=1}^{s} \Delta t_{n} \frac{\partial \boldsymbol{r}}{\partial \boldsymbol{u}} (\boldsymbol{u}_{n,i}, \boldsymbol{\mu}, t_{n-1} + c_{i} \Delta t_{n})^{T} \boldsymbol{\kappa}_{n,i}$$
$$\boldsymbol{M}^{T} \boldsymbol{\kappa}_{n,i} = \frac{\partial \boldsymbol{F}}{\partial \boldsymbol{u}_{N_{t}}}^{T} + b_{i} \boldsymbol{\lambda}_{n} + \sum_{j=i}^{s} a_{ji} \Delta t_{n} \frac{\partial \boldsymbol{r}}{\partial \boldsymbol{u}} (\boldsymbol{u}_{n,j}, \boldsymbol{\mu}, t_{n-1} + c_{j} \Delta t_{n})^{T} \boldsymbol{\kappa}_{n,j}$$

Gradient reconstruction via dual variables

$$DF = \frac{\partial F}{\partial \mu} + \lambda_0^T \frac{\partial g}{\partial \mu}(\mu) + \sum_{n=1}^{N_t} \Delta t_n \sum_{i=1}^s \kappa_{n,i}^T \frac{\partial r}{\partial \mu}(\boldsymbol{u}_{n,i}, \ \boldsymbol{\mu}, \ t_{n,i})$$

[Zahr and Persson, 2016]

Energy = 9.4096	Energy = 4.9476	Energy = 4.6182
Thrust = 0.1766	Thrust = 2.500	Thrust = 2.500

Initial Guess	Optimal RBM	Optimal $\operatorname{RBM}/\operatorname{TMG}$
	$T_x = 2.5$	$T_x = 2.5$

$$\label{eq:Energy} \begin{split} Energy &= 1.4459 e\text{-}01 \\ Thrust &= -1.1192 e\text{-}01 \end{split}$$

 $\begin{array}{l} {\rm Energy} = 3.1378 \text{e-}01 \\ {\rm Thrust} = 0.0000 \text{e+}00 \end{array}$



Experimental setup

Noisy, low-resolution MRI data

Goal: visualize *in vivo* flow with high-resolution and accurately compute clinically relevant quantities from quick scans

Idea: determine CFD parameters (material properties, boundary conditions) such that the simulation matches MRI data using optimization

$$\underset{\boldsymbol{\mu}}{\text{minimize}} \quad \sum_{i=1}^{n_{xyz}} \sum_{n=1}^{n_t} \frac{\alpha_{i,n}}{2} \left| \left| \boldsymbol{d}_{i,n}(\boldsymbol{U}(\boldsymbol{\mu}),\,\boldsymbol{\mu}) - \boldsymbol{d}_{i,n}^* \right| \right|_2^2 \right.$$

 $d^*_{i,n}$: MRI measurement taken in voxel *i* at the *n*th time sample $d_{i,n}(U, \mu)$: computational representation of $d^*_{i,n}$

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$$\begin{aligned} \boldsymbol{d}_{i,n}(\boldsymbol{U},\,\boldsymbol{\mu}) &= \int_0^T \int_V w_{i,n}(\boldsymbol{x},\,t) \cdot \boldsymbol{U}(\boldsymbol{x},\,t) \, dV \, dt \\ w_{i,n}(\boldsymbol{x},\,t) &= \chi_s(\boldsymbol{x};\,\boldsymbol{x}_i,\,\Delta \boldsymbol{x}) \chi_t(t;\,t_n,\,\Delta t) \\ \chi_t(s;\,c,\,w) &= \frac{1}{1 + e^{-(s - (c - 0.5w))/\sigma}} - \frac{1}{1 + e^{-(s - (c + 0.5w))/\sigma}} \\ \chi_s(\boldsymbol{x};\,\boldsymbol{c},\,\boldsymbol{w}) &= \chi_t(x_1;\,c_1,\,w_1) \chi_t(x_2;\,c_2,\,w_2) \chi_t(x_3;\,c_3,\,w_3) \end{aligned}$$

 \boldsymbol{x}_i center of *i*th MRI voxel, $\Delta \boldsymbol{x}$ size of MRI voxel

 t_n time instance of nth MRI sample, Δt sampling interval in time



Viscous wall (—), parametrized inflow (—), and outflow (—). MRI data collected in the red shaded region.

High-quality reconstruction from coarse MRI grid (space: 24×36 , time: 10) and low noise (3%)

Reconstructed flow

Synthetic MRI data $d_{i,n}^*$ (top) and computational representation of MRI data $d_{i,n}$ (bottom)

High-quality reconstruction from fine MRI grid (space: 40×60 , time: 20) and high noise (10%)

Reconstructed flow

Synthetic MRI data $d_{i,n}^*$ (top) and computational representation of MRI data $d_{i,n}$ (bottom) CFD-based reconstruction from quick, low-resolution scan matches laser PIV measurements better than slow, high-resolution scan

MRI data

Reconstructed flow

Extension: Parametrized time domain [Wang et al., 2017]

Parametrization of time domain, e.g., flapping frequency, leads to parametrization of time discretization in fully discrete setting

$$T(\boldsymbol{\mu}) = N_t \Delta t \implies N_t = N_t(\boldsymbol{\mu}) \text{ or } \Delta t = \Delta t(\boldsymbol{\mu})$$

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Does not change adjoint equations themselves, only reconstruction of gradient from adjoint solution

Energetically optimal flapping vs. required thrust

Energy	=	1.8445
Thrust	=	0.06729

Energy = 0.21934Thrust = 0.0000

Energy = 6.2869Thrust = 2.5000

Initial Guess	Optimal	Optimal
	$T_x = 0$	$T_x = 2.5$

For problems that involve the interaction of multiple types of physical phenomena, *no changes required* if monolithic system considered

$$egin{aligned} m{M}_0 \dot{m{u}}_0 &= m{r}_0(m{u}_0,\,m{c}_0(m{u}_0,\,m{u}_1)) \ m{M}_1 \dot{m{u}}_1 &= m{r}_1(m{u}_1,\,m{c}_1(m{u}_0,\,m{u}_1)) \end{aligned}$$

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Adjoint equations inherit explicit-implicit structure

High-order method for general multiphysics problems with unconditional linear stability

Particle-laden flow

Fluid-structure interaction

Optimal energy harvesting from foil-damper system

Goal: Maximize energy harvested from foil-damper system

$$\underset{\boldsymbol{\mu}}{\text{maximize}} \quad \frac{1}{T} \int_0^T (c\dot{h}^2(\boldsymbol{u}^s) - M_z(\boldsymbol{u}^f)\dot{\theta}(\boldsymbol{\mu}, t)) dt$$

- Fluid: Isentropic Navier-Stokes on deforming domain (ALE)
- $\bullet\,$ Structure: Force balance in y-direction between foil and damper
- Motion driven by imposed $\theta(\mu, t) = \mu_1 \cos(2\pi f t)$



High-order methods for PDE-constrained optimization

- Developed **fully discrete adjoint method** for **high-order** numerical discretizations of PDEs and QoIs
- Used to compute **gradients** of QoI for use in gradient-based numerical optimization method
- Treatment of **parametrized time domain** (optimal frequency)
- Explicit enforcement of **time-periodicity constraints**
- Extension to **multiphysics** (fluid-structure interaction, particle-laden flow, ...)
- Applications: optimal flapping flight, energy harvesting, data assimilation

Optimize physics

Optimize numerics
Supersnoic and transonic flow around commercial planes and fighter jets Hypersonics, e.g., re-entry of vehicles in atmosphere, and scramjets



Other applications with discontinuities: fracture, problems with interfaces





















<u>Fundamental issue</u>: approximate discontinuity with polynomial basis Exising solutions: limiting, artificial viscosity

Drawbacks: order reduction, local refinement

 $\underline{\text{Proposed solution:}} \text{ align features of solution basis with features in the solution using optimization formulation and solver}$



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Tracking method for stable, high-order resolution of discontinuities

<u>Goal</u>: Align element faces with (unknown) discontinuities to perfectly capture them and approximate smooth regions to high-order



Non-aligned



Discontinuity-aligned

Tracking method for stable, high-order resolution of discontinuities

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Ingredients

- Discontinuous Galerkin discretization: inter-element jumps, high-order
- Optimization formulation that penalizes local instabilities in the solution and enforces the discrete PDE
- Full space solver that converges the solution and mesh simultaneously to ensure solution of PDE never required on non-aligned mesh

 $\begin{array}{ll} \underset{\boldsymbol{u},\boldsymbol{x}}{\text{minimize}} & f(\boldsymbol{u},\,\boldsymbol{x}) \\ \text{subject to} & \boldsymbol{r}(\boldsymbol{u},\,\boldsymbol{x}) = 0 \end{array}$

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Objective function

Must obtain minimum when mesh face aligned with shock and monotonically decreases to minimum in neighborhood of radius O(h/2) about discontinuity

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Optimization approach

Cannot use **nested** approach where constraint r(u, x) = 0 is eliminated because discrete PDE cannot be solved unless $x = x^* \implies$ full space approach required

Transformed conservation law from deformation of physical domain

Consider physical domain as the result of a $\mu\text{-}\mathrm{parametrized}$ diffeomorphism applied to some reference domain Ω_0

$$\Omega = \mathcal{G}(\Omega_0, \mu)$$

Re-write conservation law on reference domain

$$\nabla \cdot \mathcal{F}(U) = 0 \quad \text{in } \mathcal{G}(\Omega_0, \mu) \implies \nabla_X \cdot F(u, \mu) = 0 \quad \text{in } \Omega_0,$$
$$u = g_\mu U, \quad F(u, \mu) = g_\mu \mathcal{F}(g_\mu^{-1} u) G_\mu^{-T}, \quad G_\mu = \frac{\partial}{\partial X} \mathcal{G}(X, \mu), \quad g_\mu = \det G_\mu$$



Mapping between reference and physical domains

Discontinuous Galerkin discretization of conservation law

Element-wise weak form of transformed conservation law

$$\int_{\partial K} \psi \cdot F(u, \mu) N \, dA - \int_K F(u, \mu) : \nabla_X \psi \, dV = 0$$

Global weak form and introduction of numerical flux

$$\sum_{K \in \mathcal{E}_{h,p}} \int_{\partial K} \psi \cdot F^*(u,\,\mu,\,N) \, dA - \int_{\Omega_0} F(u,\,\mu) : \nabla_X \psi \, dV = 0$$

Strict requirements on numerical flux since inter-element jumps will not tend to zero on shock surface



Fully discrete transformed conservation law in terms of the discrete state vector \boldsymbol{u} and coordinates of physical mesh \boldsymbol{x}

$$\boldsymbol{r}(\boldsymbol{u},\,\boldsymbol{x})=0$$

Consider a discontinuity indicator that aims to penalize oscillations in finite-dimensional solution

$$f_{shk}(\boldsymbol{u},\,\boldsymbol{x}) = h_0^{-2} \sum_{K \in \mathcal{E}_{h,p}} \int_{\mathcal{G}(K,\,\boldsymbol{x})} \left| \left| u_{h,p} - \bar{u}_{h,p}^K \right| \right|_{\boldsymbol{W}}^2 \, dV,$$

$$\bar{u}_{h,p}^{K} = \frac{1}{|\mathcal{G}(K, \boldsymbol{x})|} \int_{\mathcal{G}(K, \boldsymbol{x})} u_{h,p} \, dV, \qquad |\mathcal{G}(K, \boldsymbol{x})| = \int_{\mathcal{G}(K, \boldsymbol{x})} dV, \qquad h_0 = |\Omega_0|^{1/d}$$

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Construct objective function as weighted combination between discontinuity indicator and mesh distortion metric

$$f(\boldsymbol{u}, \boldsymbol{x}; \alpha) = f_{shk}(\boldsymbol{u}, \boldsymbol{x}) + \alpha f_{msh}(\boldsymbol{x})$$















$$j_{\alpha}(\boldsymbol{\phi}) = f_{shk}(\boldsymbol{u}(\boldsymbol{x}(\boldsymbol{\phi})), \, \boldsymbol{x}(\boldsymbol{\phi})) + \alpha f_{msh}(\boldsymbol{x}(\boldsymbol{\phi}))$$

Objective function as an element face is smoothly swept across discontinuity (---): p = 1 (--), p = 2 (--), p = 3 (--), p = 4 (--).



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Proposed discontinuity indicator is monotonic and attains minimum at discontinuity, whereas other indicators are not monotonic



Objective function as an element face is smoothly swept across discontinuity (- - -): p = 1 (---), p = 2 (---), p = 3 (---). Proposed discontinuity indicator is monotonic and attains minimum at discontinuity, whereas other indicators are not monotonic



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Objective function as an element face is smoothly swept across discontinuity (---): p = 1 (--), p = 2 (--), p = 3 (--).
Cannot use nested approach to PDE optimization because it requires solving r(u, x) = 0 for $x \neq x^* \implies$ crash

Full space approach: $u \to u^*$ and $x \to x^*$ simultaneously

¹usually requires globalization such as linesearch or trust-region

Cannot use nested approach to PDE optimization because it requires solving r(u, x) = 0 for $x \neq x^* \implies$ crash

Full space approach: $u \to u^*$ and $x \to x^*$ simultaneously Define Lagrangian

$$\mathcal{L}(\boldsymbol{u}, \boldsymbol{x}, \boldsymbol{\lambda}) = f(\boldsymbol{u}; \boldsymbol{x}) - \boldsymbol{\lambda}^T \boldsymbol{r}(\boldsymbol{u}; \boldsymbol{x})$$

First-order optimality (KKT) conditions for full space optimization problem

$$abla_{oldsymbol{u}}\mathcal{L}(oldsymbol{u}^*,oldsymbol{x}^*,oldsymbol{\lambda}^*)=oldsymbol{0},\qquad
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Apply (quasi-)Newton method¹ to solve nonlinear KKT system for $u^*, \, x^*, \, \lambda^*$

¹usually requires globalization such as linesearch or trust-region

Gradient-based optimizers for the tracking optimization problem will require

- r and $\partial_u r$ required by standard implicit solvers
- Same terms required for reduced space approach

L^2 projection of discontinuous function on DG basis



Non-aligned (left) vs. discontinuity-aligned mesh with linear (middle) and cubic (right) elements





Resolution of modified Burgers' equation with few elements





Convergence: tracking vs. uniform/adaptive refinement





Inviscid wall (---), inflow (---), outflow (---)

Resolution of quasi-1d Euler equations with few elements



Exact solution (-----), tracking solution (-----) and mesh (-----) for p = 3

Resolution of quasi-1d Euler equations with few elements



Exact solution (-----), tracking solution (-----) and mesh (-----) for p = 3

Resolution of quasi-1d Euler equations with few elements



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 $p = 1 (\bullet), p = 2 (\blacksquare)$ Slope of best-fit line: $\angle -2.0 (---), \angle -2.7 (---)$ Reference second-order method (p = 1) with adaptive mesh refinement (**x**)



Density (ρ)



Left: Solution on non-aligned mesh with 48 linear elements and added viscosity (initial guess for shock tracking method). Remaining: solution using shock tracking framework corresponding to mesh with 48 p = 1, p = 2, p = 3, p = 4 elements.

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Shock tracking objective (f_{shk})



Left: Solution on non-aligned mesh with 48 linear elements and added viscosity (initial guess for shock tracking method). Remaining: solution using shock tracking framework corresponding to mesh with 48 p = 1, p = 2, p = 3, p = 4 elements.

Distortion metric (f_{msh})



Left: Solution on non-aligned mesh with 48 linear elements and added viscosity (initial guess for shock tracking method). *Remaining:* solution using shock tracking framework corresponding to mesh with 48 p = 1, p = 2, p = 3, p = 4 elements.

Polynomial order (p)	1	2	3	4
Degrees of freedom (N_u)	576	1152	1920	2880
Enthalpy error (e_H)	0.0106	0.000462	0.00151	0.000885
Stagnation pressure error (e_p)	0.0711	0.00479	0.0112	0.000616



Resolution of 2D supersonic flow with 102 quadratic elements



Left: Solution (density) on non-aligned mesh with 102 linear elements and added viscosity (initial guess for shock tracking method). *Middle/right:* solution using shock tracking framework corresponding to mesh with 102 linear (*middle*) and quadratic (*right*) elements.

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Left: Solution (density) on non-aligned mesh with 102 linear elements and added viscosity (initial guess for shock tracking method). *Middle/right:* solution using shock tracking framework corresponding to mesh with 102 linear (*middle*) and quadratic (*right*) elements.



Convergence of residual and objective function

Conclusions and future work

- Introduced high-order shock tracking method based on DG discretization and PDE-constrained optimization formulation
- Key innovations: *objective function* that monotonically approaches a minimum as mesh face aligns with shock and *full space solver*
- Optimal convergence $\mathcal{O}(h^{p+1})$ rates obtained and used to resolve a number of transonic and supersonic flows on very coarse meshes
- Future work
 - numerical flux consistent with *integral form* (jumps do not tend to 0)
 - solver that exploits *problem structure* and incorporates *homotopy*
 - local topology changes to reduce iterations and improve mesh quality



Mach 2 flow around cylinder (*left*), Mach 4 flow around blunt body (*middle*), and L^2 projection of discontinuous function (*right*).

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PDE optimization is ubiquitous in science and engineering

Control: Drive system to a desired state



Boundary flow control



Metamaterial cloaking – electromagnetic invisibility

• Continuous PDE-constrained optimization problem

$$\begin{split} \underset{\boldsymbol{U}, \ \boldsymbol{\mu}}{\text{minimize}} & \mathcal{J}(\boldsymbol{U}, \boldsymbol{\mu}) \\ \text{subject to} & \boldsymbol{C}(\boldsymbol{U}, \boldsymbol{\mu}) \leq 0 \\ & \frac{\partial \boldsymbol{U}}{\partial t} + \nabla \cdot \boldsymbol{F}(\boldsymbol{U}, \nabla \boldsymbol{U}) = 0 \ \text{ in } \ \boldsymbol{v}(\boldsymbol{\mu}, t) \end{split}$$

• Fully discrete PDE-constrained optimization problem

$$\begin{array}{l} \underset{u_{0}, \ldots, u_{N_{t}} \in \mathbb{R}^{N_{u}}, \\ k_{1,1}, \ldots, k_{N_{t},s} \in \mathbb{R}^{N_{u}}, \\ \mu \in \mathbb{R}^{n_{\mu}} \end{array} \qquad J(u_{0}, \ \ldots, \ u_{N_{t}}, \ k_{1,1}, \ \ldots, \ k_{N_{t},s}, \ \mu) \\ \text{subject to} \qquad \mathbf{C}(u_{0}, \ \ldots, \ u_{N_{t}}, \ k_{1,1}, \ \ldots, \ k_{N_{t},s}, \ \mu) \leq 0 \\ u_{0} - g(\mu) = 0 \\ u_{n} - u_{n-1} - \sum_{i=1}^{s} b_{i} k_{n,i} = 0 \\ \mathbf{M} k_{n,i} - \Delta t_{n} r(u_{n,i}, \ \mu, \ t_{n,i}) = 0 \end{array}$$

Let $u(\mu)$ be the solution of $r(\cdot, \mu) = 0$

$$\boldsymbol{r}(\boldsymbol{\mu}) = \boldsymbol{r}(\boldsymbol{u}(\boldsymbol{\mu}), \boldsymbol{\mu}) = 0, \qquad F(\boldsymbol{\mu}) = F(\boldsymbol{u}(\boldsymbol{\mu}), \boldsymbol{\mu})$$

Let $u(\mu)$ be the solution of $r(\cdot, \mu) = 0$

$$\boldsymbol{r}(\boldsymbol{\mu}) = \boldsymbol{r}(\boldsymbol{u}(\boldsymbol{\mu}), \boldsymbol{\mu}) = 0, \qquad F(\boldsymbol{\mu}) = F(\boldsymbol{u}(\boldsymbol{\mu}), \boldsymbol{\mu})$$

The total derivative of r leads to the sensitivity equations

$$Dr = \frac{\partial r}{\partial \mu} + \frac{\partial r}{\partial u} \frac{\partial u}{\partial \mu} = 0 \implies \frac{\partial u}{\partial \mu} = -\frac{\partial r}{\partial u}^{-1} \frac{\partial r}{\partial \mu}$$

Let $u(\mu)$ be the solution of $r(\cdot, \mu) = 0$

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The total derivative of r leads to the sensitivity equations

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The total derivative of F

$$DF = \frac{\partial F}{\partial \mu} + \frac{\partial F}{\partial u} \frac{\partial u}{\partial \mu}$$

Let $u(\mu)$ be the solution of $r(\cdot, \mu) = 0$

$$\boldsymbol{r}(\boldsymbol{\mu}) = \boldsymbol{r}(\boldsymbol{u}(\boldsymbol{\mu}), \boldsymbol{\mu}) = 0, \qquad F(\boldsymbol{\mu}) = F(\boldsymbol{u}(\boldsymbol{\mu}), \boldsymbol{\mu})$$

The total derivative of r leads to the sensitivity equations

$$D\boldsymbol{r} = \frac{\partial \boldsymbol{r}}{\partial \boldsymbol{\mu}} + \frac{\partial \boldsymbol{r}}{\partial \boldsymbol{u}} \frac{\partial \boldsymbol{u}}{\partial \boldsymbol{\mu}} = 0 \implies \frac{\partial \boldsymbol{u}}{\partial \boldsymbol{\mu}} = -\frac{\partial \boldsymbol{r}}{\partial \boldsymbol{u}}^{-1} \frac{\partial \boldsymbol{r}}{\partial \boldsymbol{\mu}}$$

The total derivative of F

$$DF = \frac{\partial F}{\partial \mu} + \frac{\partial F}{\partial u} \frac{\partial u}{\partial \mu} = \frac{\partial F}{\partial \mu} - \frac{\partial F}{\partial u} \frac{\partial r}{\partial u}^{-1} \frac{\partial r}{\partial \mu}$$
Discrete adjoint equations can be derived from an algebraic manipulation to save computations

Let $u(\mu)$ be the solution of $r(\cdot, \mu) = 0$

$$\boldsymbol{r}(\boldsymbol{\mu}) = \boldsymbol{r}(\boldsymbol{u}(\boldsymbol{\mu}), \boldsymbol{\mu}) = 0, \qquad F(\boldsymbol{\mu}) = F(\boldsymbol{u}(\boldsymbol{\mu}), \boldsymbol{\mu})$$

The total derivative of r leads to the sensitivity equations

$$Dr = \frac{\partial r}{\partial \mu} + \frac{\partial r}{\partial u} \frac{\partial u}{\partial \mu} = 0 \implies \frac{\partial u}{\partial \mu} = -\frac{\partial r}{\partial u}^{-1} \frac{\partial r}{\partial \mu}$$

The total derivative of F

$$DF = \frac{\partial F}{\partial \mu} + \frac{\partial F}{\partial u}\frac{\partial u}{\partial \mu} = \frac{\partial F}{\partial \mu} - \frac{\partial F}{\partial u}\frac{\partial r}{\partial u}^{-1}\frac{\partial r}{\partial \mu} = \frac{\partial F}{\partial \mu} - \lambda^{T}\frac{\partial r}{\partial \mu}$$

Discrete adjoint equations can be derived from an algebraic manipulation to save computations

Let $u(\mu)$ be the solution of $r(\cdot, \mu) = 0$

$$\boldsymbol{r}(\boldsymbol{\mu}) = \boldsymbol{r}(\boldsymbol{u}(\boldsymbol{\mu}), \boldsymbol{\mu}) = 0, \qquad F(\boldsymbol{\mu}) = F(\boldsymbol{u}(\boldsymbol{\mu}), \boldsymbol{\mu})$$

The total derivative of r leads to the sensitivity equations

$$D\boldsymbol{r} = \frac{\partial \boldsymbol{r}}{\partial \boldsymbol{\mu}} + \frac{\partial \boldsymbol{r}}{\partial \boldsymbol{u}} \frac{\partial \boldsymbol{u}}{\partial \boldsymbol{\mu}} = 0 \implies \frac{\partial \boldsymbol{u}}{\partial \boldsymbol{\mu}} = -\frac{\partial \boldsymbol{r}}{\partial \boldsymbol{u}}^{-1} \frac{\partial \boldsymbol{r}}{\partial \boldsymbol{\mu}}$$

The total derivative of F

$$DF = \frac{\partial F}{\partial \mu} + \frac{\partial F}{\partial u} \frac{\partial u}{\partial \mu} = \frac{\partial F}{\partial \mu} - \frac{\partial F}{\partial u} \frac{\partial r}{\partial u}^{-1} \frac{\partial r}{\partial \mu} = \frac{\partial F}{\partial \mu} - \lambda^T \frac{\partial r}{\partial \mu}$$

Algebraic equations leads to adjoint equations

$$\frac{\partial \boldsymbol{r}}{\partial \boldsymbol{u}}^{T} \boldsymbol{\lambda} = \frac{\partial F}{\partial \boldsymbol{u}}^{T}$$

$$\frac{\partial F}{\partial \boldsymbol{u}} \frac{\partial \boldsymbol{r}}{\partial \boldsymbol{u}}^{-1} \frac{\partial \boldsymbol{r}}{\partial \boldsymbol{\mu}}$$







Sensitivity method requires n_{μ} linear solves and $n_F n_{\mu}$ inner products (\mathbb{R}^{n_u})

$$\frac{\partial F}{\partial \boldsymbol{u}} \frac{\partial \boldsymbol{r}}{\partial \boldsymbol{u}}^{-1} \frac{\partial \boldsymbol{r}}{\partial \boldsymbol{\mu}}$$



Sensitivity method requires n_{μ} linear solves and $n_F n_{\mu}$ inner products (\mathbb{R}^{n_u})

$$\frac{\partial F}{\partial \boldsymbol{u}} \frac{\partial \boldsymbol{r}}{\partial \boldsymbol{u}}^{-1} \frac{\partial \boldsymbol{r}}{\partial \boldsymbol{\mu}}$$



Sensitivity method requires n_{μ} linear solves and $n_F n_{\mu}$ inner products (\mathbb{R}^{n_u}) Adjoint method requires n_F linear solves and $n_F n_{\mu}$ inner products (\mathbb{R}^{n_u})

Adjoint equation derivation: outline

• Define **auxiliary** PDE-constrained optimization problem

$$\begin{array}{l} \underset{u_{0}, \dots, u_{N_{t}} \in \mathbb{R}^{N_{u}}, \\ k_{1,1}, \dots, k_{N_{t},s} \in \mathbb{R}^{N_{u}} \end{array}}{\text{minimize}} \quad F(u_{0}, \dots, u_{N_{t}}, k_{1,1}, \dots, k_{N_{t},s}, \mu) \\ \text{subject to} \quad R_{0} = u_{0} - g(\mu) = 0 \\ R_{n} = u_{n} - u_{n-1} - \sum_{i=1}^{s} b_{i}k_{n,i} = 0 \\ R_{n,i} = Mk_{n,i} - \Delta t_{n}r(u_{n,i}, \mu, t_{n,i}) = 0 \end{array}$$

• Define Lagrangian

$$\mathcal{L}(\boldsymbol{u}_n, \boldsymbol{k}_{n,i}, \boldsymbol{\lambda}_n, \boldsymbol{\kappa}_{n,i}) = F - \boldsymbol{\lambda}_0^T \boldsymbol{R}_0 - \sum_{n=1}^{N_t} \boldsymbol{\lambda}_n^T \boldsymbol{R}_n - \sum_{n=1}^{N_t} \sum_{i=1}^s \boldsymbol{\kappa}_{n,i}^T \boldsymbol{R}_{n,i}$$

• The solution of the optimization problem is given by the Karush-Kuhn-Tucker (KKT) sytem

$$\frac{\partial \mathcal{L}}{\partial u_n} = 0, \quad \frac{\partial \mathcal{L}}{\partial k_{n,i}} = 0, \quad \frac{\partial \mathcal{L}}{\partial \lambda_n} = 0, \quad \frac{\partial \mathcal{L}}{\partial \kappa_{n,i}} = 0$$

High-quality reconstruction from coarse MRI grid (space: 24×36 , time: 20) and low noise (3%)

Reconstructed flow

Synthetic MRI data $d_{i,n}^*$ (top) and computational representation of MRI data $d_{i,n}$ (bottom)

High-quality reconstruction from fine MRI grid (space: 40×60 , time: 20) and low noise (3%)

Reconstructed flow

Synthetic MRI data $d_{i,n}^*$ (top) and computational representation of MRI data $d_{i,n}$ (bottom)

Extension: constraint requiring time-periodicity [Zahr et al., 2016]

Optimization of *cyclic* problems requires finding time-periodic solution of PDE; necessary for physical relevance and avoid transients that may lead to crash



Time history of power on airfoil of flow initialized from steady-state (--) and from a time-periodic solution (--)

Energetically optimal flapping vs. required thrust: QoI



The optimal flapping energy (W^*) , frequency (f^*) , maximum heaving amplitude (y^*_{\max}) , and maximum pitching amplitude (θ^*_{\max}) as a function of the thrust constraint \bar{T}_x .

- Initial guess for u and ϕ critical given the non-convex nonlinear optimization formulation of our shock tracking method
- Homotopy: define a sequence of shock tracking problems where the solution of problem j is used to initialize problem j + 1
- Sequence of problems chosen using homotopy in *polynomial order* and Mach number (for high Mach flows)
- For initial problem in homotopy sequence:
 - ϕ_0 chosen such that resulting mesh is identical to the reference mesh
 - u_0 chosen as the solution of the discrete conservation law with enough added viscosity ν

$$\boldsymbol{r}_{\nu}(\boldsymbol{u},\,\boldsymbol{x}(\boldsymbol{\phi}_{0}))=0$$

Inviscid, modified one-dimensional Burgers' equation with a discontinuous source term from [Barter, 2008]

$$\frac{\partial}{\partial x}\left(\frac{1}{2}u^2\right) = \beta u + f(x), \quad \text{for } x \in \Omega = (-2, 2),$$

where u(-2) = 2, u(2) = -2, $\beta = -0.1$ and

$$f(x) = \begin{cases} (2 + \sin(\frac{\pi x}{2}))(\frac{\pi}{2}\cos(\frac{\pi x}{2}) - \beta), & x < 0\\ (2 + \sin(\frac{\pi x}{2}))(\frac{\pi}{2}\cos(\frac{\pi x}{2}) + \beta), & x > 0 \end{cases}$$

Analytical solution

$$u(x) = \begin{cases} 2 + \sin(\frac{\pi x}{2}), & x < 0\\ -2 - \sin(\frac{\pi x}{2}), & x > 0 \end{cases}$$



Reference domain and mesh with 48 elements and polynomial orders p = 1 (*left*), p = 2 (*middle left*), p = 3 (*middle right*), and p = 4 (*right*). The blue circles identify parametrized nodes.